

Advances in Smartphone-Based Point-of-Care Diagnostics

This paper reviews the state-of-the-art advances in smartphone-based point-of-care diagnostic technologies and their applications in medicine and biology.

By XIAYU XU, ALTUG AKAY, HUILIN WEI, SHUQI WANG, BELINDA PINGGUAN-MURPHY, BJÖRN-ERIK ERLANDSSON, XIUJUN LI, WONGU LEE, JIE HU, LIN WANG, AND FENG XU

ABSTRACT | Point-of-care (POC) diagnostics is playing an increasingly important role in public health, environmental monitoring, and food safety analysis. Smartphones, alone or in conjunction with add-on devices, have shown great capability of data collection, analysis, display, and transmission, making them popular in POC diagnostics. In this article, the state-of-the-art advances in smartphone-based POC diagnostic technologies and their applications in the past few years are outlined, ranging from *in vivo* tests that use smartphone's built-in/external sensors to detect biological signals to *in vitro* tests that involves complicated biochemical reactions. Novel

techniques are illustrated by a number of attractive examples, followed by a brief discussion of the smartphone's role in telemedicine. The challenges and perspectives of smartphone-based POC diagnostics are also provided.

KEYWORDS | Mobile medicine; point-of-care (POC) diagnostics; public health; smartphone

I. INTRODUCTION

As a form of test performed at or near the test site, point-of-care (POC) diagnostics has received increasing attention in recent years [1]–[9]. POC diagnostics offers several advantages compared with laboratory-based tests in that the former is normally portable, inexpensive, rapid, and easy-to-use [10]. These features have provided POC diagnostics with an indispensable role in global and public health, such as in the control and treatment of infectious and chronic diseases [11]–[13]. For example, it can provide timely diagnostics for tuberculosis (TB) and human immunodeficiency virus (HIV), effectively preventing the spread of these diseases, and provide continuous, long-term monitoring services for diabetes mellitus and cardiovascular diseases [14]–[17]. Besides, POC diagnostics has shown great potential in environmental monitoring and food safety analysis [18], [19]. Therefore, the development of POC diagnostic technologies becomes increasingly urgent.

The three phases of a POC test are preanalytical, analytical, and postanalytical [20]. Preanalytical phase includes selection of proper test methods and specimen collection. Analytical phase is the process of detecting targeted biological signals and transforming them into measurable signals. Postanalytical phase includes data analysis, result display, storage and transmission, and decision-making. Early POC technologies usually require extra peripheral devices for analytical and postanalytical evaluation (e.g., electronic sphygmomanometer), thus significantly increasing the cost and complexity in performance and limiting

Manuscript received July 1, 2014; revised October 29, 2014; accepted November 21, 2014. Date of current version March 23, 2015. This work was financially supported by the National 111 Project of China (B06024), the Key (Key grant) Project of Chinese Ministry of Education (313045), South Wisdom Valley Innovative Research Team Program, International Science & Technology Cooperation Program of China (2013DFG02930), Key Program for International S&T Cooperation Projects of Shaanxi (2014KW12-01), the Fundamental Research Funds for the Central Universities, National Natural Science Foundation of China (81401480), and China Postdoctoral Science Foundation (2013M532054, 2014M552460). B.P.-M. received funding from the Ministry of Higher Education (MOHE), Government of Malaysia, under the high impact research grant (UM.C/HIR/MOHE/ENG/44).

X. Xu, J. Hu, L. Wang, and F. Xu are with the MOE Key Laboratory of Biomedical Information Engineering, School of Life Science and Technology, Xi'an Jiaotong University, Xi'an, China. They are also with the Bioinspired Engineering and Biomechanics Center (BEBC), Xi'an Jiaotong University, Xi'an, China (e-mail: wanglin0527@126.com; changjie.hu@gmail.com).

A. Akay and B.-E. Erlandsson are with the School of Technology and Health, Royal Institute of Technology, Huddinge, SE-141 52 Sweden.

H. Wei is with the Novatein Biosciences, Inc., Woburn, MA, 01801 USA.

S. Wang is with the MOE Key Laboratory of Biomedical Information Engineering, School of Life Science and Technology, Xi'an Jiaotong University, Xi'an, China. He is also with the Bio-Acoustic MEMS in Medicine (BAMM) Laboratory, Canary Center at Stanford for Cancer Early Detection, Department of Radiology, Stanford School of Medicine, Palo Alto, CA 94304 USA. He is also with the State Key Laboratory for Diagnosis and Treatment of Infectious Diseases, First Affiliated Hospital, College of Medicine, Zhejiang University, Hangzhou, China, and with the Collaborative Innovation Center for Diagnosis and Treatment of Infectious Diseases, Hangzhou, China, and also with the Institute for Translational Medicine, Zhejiang University, Hangzhou, China.

B. Pingguan-Murphy is with the Department of Biomedical Engineering, Faculty of Engineering, University of Malaya, Kuala Lumpur 50603, Malaysia.

X. Li is with the Border Biomedical Research Center, Biomedical Engineering (BME) and Material Science and Engineering (MASE), University of Texas at El Paso, El Paso, TX 79902 USA.

W. Lee is with the Department of Mechanical Engineering, Kyung Hee University, Korea.

Digital Object Identifier: 10.1109/JPROC.2014.2378776

0018-9219 © 2015 IEEE. Personal use is permitted, but republication/redistribution requires IEEE permission. See http://www.ieee.org/publications_standards/publications/rights/index.html for more information.

Table 1 Categories of Smartphone-Based Diagnostics

Category	Explanation	Examples	
<i>In vivo</i> test	Tests that do not require sample consumption; biological signals are converted to electrical signals by various sensors.	Test with built-in sensor	Use the built-in sensors, such as the camera, to collect human body or environmental signals.
		Test with extra sensor	Use extra sensors, such as an ultrasound probe, to collect human body or environmental signals.
<i>In vitro</i> test	Tests that require sample consumption; biological components or organisms are detected from samples, such as blood, sweat, <i>etc.</i>	Tube, strip, and specimen inspection	Take a specimen of bodily fluid and directly inspect the result using the built-in camera or a microscope connected to a smartphone.
		Microfluidic testing	Take a specimen of bodily fluid and use microfluidic technique to perform complicated biochemical tests, and visualize the result using a smartphone.

their widespread applications in global and public health. Developing cost-effective and easy-to-operate POC technologies is therefore desirable.

Recent advances in smartphone technologies hold great potential to solve these problems. Smartphones, equipped with a computer-like platform and various types of sensors, have several properties promoting their uses in POC diagnostics [21]. The global market has witnessed a rapid growth of smartphones in recent years. Reports from International Data Corporation (IDC) and Canalis state that the number of smartphone subscriptions worldwide has reached up to 1.0 billion in 2013, and the number is expected to surpass 1.2 billion in 2014, driven by rapid growth in developing countries (e.g., India and China) [22], [23]. This means that smartphones are becoming widely accessible even in resource-limited areas lacking adequate healthcare facilities. Furthermore, a rich set of built-in sensors (e.g., camera and microphone) can be used for the detection of biological signals, powerful processors and memories for the analysis and storage of diagnostic results, and high resolution screens for result display [24], [25]. Finally, smartphones are generally equipped with powerful data transmission capabilities, such as Global System for Mobile Communication (GSM), wireless fidelity (Wi-Fi), Bluetooth, and universal serial bus (USB), allowing short-distance and long-distance communication between a remote test site and centralized laboratory for professional guidance.

Over the past few years, there has been a significant increase in smartphone-based healthcare technologies, as reflected by over 40,000 mobile health applications available in 2012 [26]. A number of articles have reviewed these advances: Patrick *et al.* and Wang *et al.* reviewed the application of smartphone in healthcare respectively in 2008 and 2009 [27], [28]. Xie *et al.* reviewed the development of biomedical imaging techniques combined with smartphones in 2010 [29]. With the rapid development of

smartphone, many novel features are available now, and many new healthcare technologies have been introduced. A more recent review by Agu *et al.* focused on the usage of smartphone in medical condition diagnostics that takes advantage of the smartphone's built-in camera or microphone [30]. Another recent review by Ozcan *et al.* focused on the uses of smartphone for imaging/microscopy and optoelectronic/electronic sensing, such as smartphone-based microscopy that can detect single virus, as well as smartphone-based cytometry [31]. These existing reviews have not focused on the combination of smartphone and POC diagnostics or only focused on a single area of smartphone-based POC diagnostics. Here, we review the latest developments in smartphone-based POC diagnostics, ranging from *in vivo* tests that use smartphone's built-in/external sensors to detect biological signals to *in vitro* tests that are combined with complicated biochemical reactions (Table 1). Novel techniques are introduced and illustrated by a number of attractive examples, followed by a brief discussion of the smartphone's role in telemedicine. Last, we present the challenges and perspectives in smartphone-based POC diagnostics.

II. *IN VIVO* TESTING

In vivo tests capture health information from the target without sample consumption. Some biological signals, such as two-dimensional (2D) color images and sounds, can be directly captured using a smartphone. Furthermore, more sophisticated diagnostic information can be obtained by connecting smartphone with add-on devices [32], [33].

A. Smartphone-Based POC Diagnostics With Built-in Sensors

Although a variety of sensors have been imbedded in smartphone, the widely used sensors in POC diagnostics are still limited to camera and microphone. A large amount

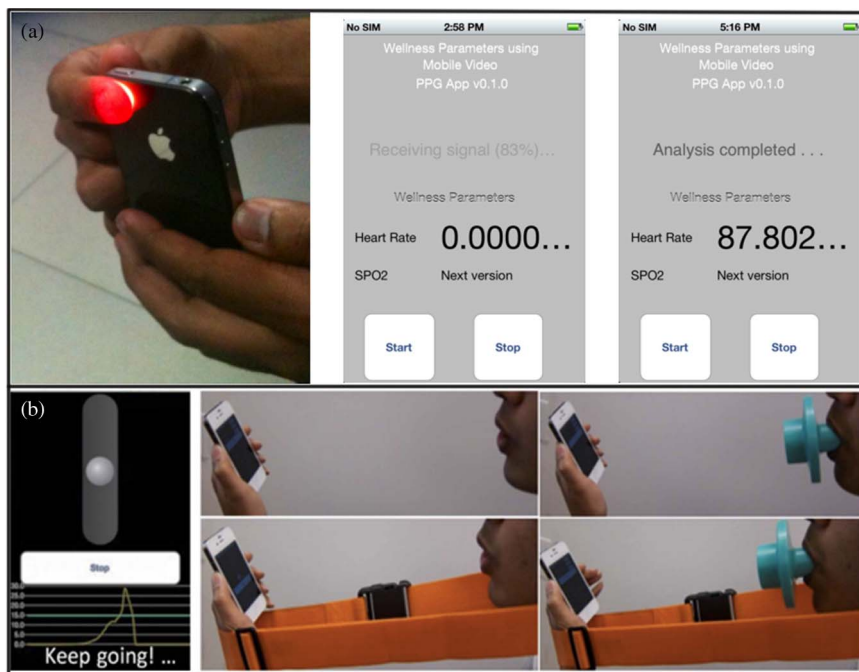


Fig. 1. Examples of *in vivo* POC diagnostics with smartphone's built-in sensors. (a) Heart rate detection from a fingertip [35]. (b) POC spirometer by recording the sound of exhalation using smartphone's built-in microphone [41].

of diagnostic information can be extracted from the raw audio or video data when combined with signal or image processing algorithms.

The megapixel count of the smartphone's built-in camera has been doubled in every two years in recent decades and is now as high as 41 megapixels (Nokia 808 Pure-View). Researchers are able to extract various types of health information from images of the human body, such as fingertips, eyes, and skin using image and/or video post-processing techniques performed either in a smartphone or computer. Widely used image processing algorithms include Fourier transform [34], [35], color signal analysis [36], region segmentation [37], and pattern recognition [38], [39]. For example, fingertips contain abundant information about blood circulation. Jonathan *et al.* [34] and Pal *et al.* [35] obtained changes in heart rate by capturing photoplethysmographic (PPG) signals from a fingertip using a reflection PPG imaging technique [Fig. 1(a)]. To collect PPG signals from a fingertip, a smartphone was used to detect, record, and process the reemitted signals of a white light emitting diode (LED) illumination source. Similarly, Scully *et al.* achieved monitoring of various physiological signals, including cardiac R-R intervals, breathing rate, and blood oxygen saturation [36].

In addition to obtaining blood circulation status from fingertips, a bunch of other smartphone-based technologies have been developed. For example, a simple smartphone-based pupilloeter was developed to measure the diameter of pupil, providing information on the function of autonomic

nervous system [37]. By comparing tongue images acquired using a smartphone with an image database, Samsung Electronics Company developed a method to determine the overall health status of a person (e.g., fatigue status) [38]. Similarly, Wadhawan *et al.* developed a smartphone-based melanoma detection technology [39].

Audio information taken by the smartphone's built-in microphone, combined with digital signal processing algorithms, is also used to acquire health information. Yoshimine *et al.* reported the use of a voice-recording function to diagnose the overall health status of individuals by comparing to the voice database from healthy individuals [40]. Larson *et al.* reported a smartphone-based spirometer, in which the sound of exhalation is recorded and analyzed for lung function [see Fig. 1(b)] [41]. Thus, smartphone-based POC technologies have been rapidly developed to collect and monitor basic health information in nonclinical settings.

B. Smartphone-Based POC Diagnostics With External Sensors

So far, the information extracted by smartphone's built-in sensors is mainly limited to images and sounds. Many external sensor systems have been designed and integrated into the smartphone to extend its capability to extract more sophisticated diagnostic information, such as body temperature and functional images of organs and tissues. This allows previously unattainable health information to be extracted using external sensors and processed or



Fig. 2. Examples of *in vivo* POC diagnostics with extra sensors. (a) Skin temperature detection by mapping skin temperature changes to TLC color changes [42]. (b) POC ultrasound imaging system (MobiSante MobiUS SP1 system) with two mechanical sector USB probes [44].

transmitted using a smartphone in the form of one-dimensional (e.g., body temperature and pulse rate), two-dimensional (e.g., ultrasound image), or three-dimensional (e.g., time-sequence ultrasound images) signals.

Huang *et al.* developed a smartphone-based thermal imaging technology to quantitatively measure the temperature of human skin [42]. In this method, liquid crystal thermal (TLC), showing temperature changes in different color, was preapplied on human skin. The color changes were then captured as two-dimensional images using a smartphone's built-in camera and analyzed in a personal computer to measure the final temperature [see Fig. 2(a)] [42]. Khandoker *et al.* developed a smartphone-based low-cost oximeter photoplethysmography [43], in which the desired information, including blood oxygen saturation and pulse rate, was collected using a hardware system that can detect the absorption of red and infrared signals through a fingertip. The digital signals were then transmitted to a smartphone through USB for diagnostic result display and data communication between on-site patients and off-site clinicians.

Smartphone-based medical imaging is an important emerging area in POC diagnostics. Medical imaging, different from smartphone-based microscopy introduced in Section III-A, is the technique applied to create images of

the human body (or function and parts) for clinical purposes, such as X-ray, computed tomography (CT), optical coherent tomography (OCT) and ultrasound. With the capability of providing high-resolution images of internal structure of human body, medical imaging has been widely used in the evaluation and diagnosis of many diseases. However, the high cost and need for highly trained skill to operate these clinical devices prohibit such imaging technologies from many remote regions. With significant advances in smartphone's display and processing capabilities, medical imaging combined with smartphone has become a research area with great potential [29]. MobiSante developed an ultrasound probe that is able to be plugged into a smartphone [Fig. 2(b)] [44]. With an ultrasonic transducer, the smartphone can acquire and display ultrasound images, which can then be transmitted to an off-site health center for further interpretation. Using this system, they obtained images of the suprahyoid airway and muscular architecture of mouth floor.

III. *IN VITRO* TESTING

In vitro tests are biochemical tests that detect/measure biological components (e.g., metabolites, proteins, and nuclei acids) and organisms (e.g., cells and microbes) from

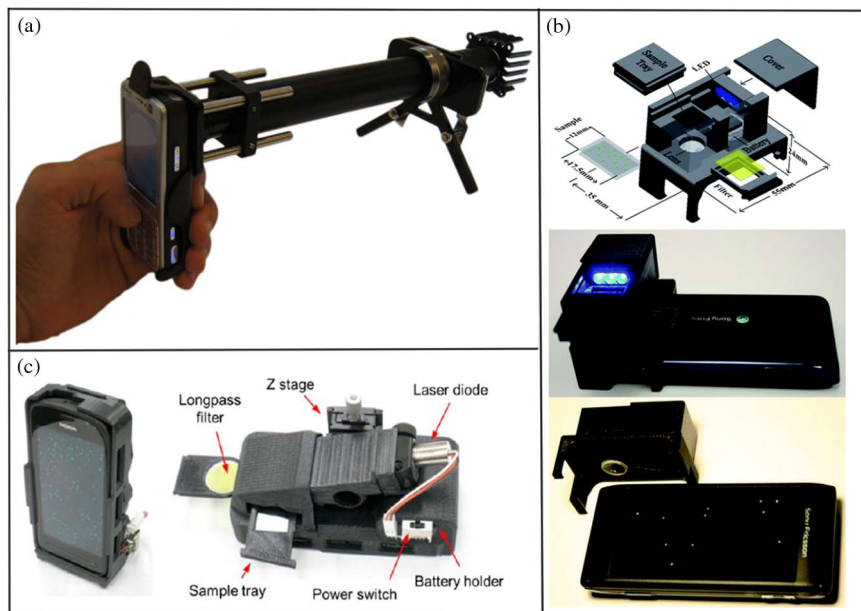


Fig. 3. Examples of smartphone-based microscopy systems. (a) Smartphone microscopy optical layout for fluorescence imaging [48]. (b) Schematic diagram and different views of the designed optical attachment for wide-field fluorescent imaging on a cell-phone [49]. (c) A cell phone-based fluorescence microscope [50].

blood, sweat, saliva, urine, water, or food [11], including conventional microscopy, widely used lateral flow assays, and lately developed microfluidic devices.

A. Recent Developments of Smartphone-Based Microscopy

Microscopy, which allows the microscale investigation of biological specimens, is widely used in biochemical tests to identify objects (e.g., cells, bacterium, and parasites) that cannot be visualized directly by naked eyes [45], [46]. Microscopes can be used in specimen tests, microfluidic tests, or any other form of *in vitro* tests that need visualization in microscale. Conventional lab microscopy is relatively costly, bulky, and requires a highly trained staff, impeding its application to near-patient diagnosis. In response, researchers have developed accurate, cost-effective, and easy-to-perform microscopy, as a general tool suitable for POC applications using smartphones. Hence, before we delve into any specific smartphone-based biochemical diagnostic technique, we briefly review the recent development in smartphone-based microscopic imaging techniques.

Most smartphone-based microscopes are optical microscopes that consist of a visible light source and a system of lenses to magnify images of small objects. Image resolution and field-of-view (FOV) are two main parameters to evaluate the optical microscope's performance. Smith *et al.* developed a microscope attached to a smartphone that transformed the phone's integrated lens to a $350\times$ microscope and visible-light spectrometer [47]. The microscope has a resolution of $1.5\ \mu\text{m}$ and a usable FOV of $150 \times$

$150\ \mu\text{m}$ without image processing and approximately $350 \times 350\ \mu\text{m}$ with postprocessing. Breslauer *et al.* reported a smartphone-mounted light microscope and obtained a resolution of $1.2\ \mu\text{m}$ and a usable FOV of $180 \times 180\ \mu\text{m}$ by adding a ball-lens to the system [see Fig. 3(a)] [48]. Zhu *et al.* demonstrated a wide-field fluorescent and dark-field imaging technique on a smartphone, in which a specimen was excited by a battery powered LED, after which the fluorescent emission from the sample was imaged using an additional lens positioned in front of the built-in camera [see Fig. 3(b)] [49]. This smartphone-based microscopy showed a large FOV of $\sim 81\ \text{mm}^2$ with a raw spatial resolution of $\sim 10\ \mu\text{m}$. Wei *et al.* reported a field-portable fluorescence microscopy platform installed on a smartphone with high spatial resolution that is able to image both individual nanoparticles (100 nm of fluorescent particles) and viruses (fluorescently labeled human cytomegaloviruses) [see Fig. 3(c)] [50].

A type of lens-free microscope has been recently developed that obviates the need for any lenses or other optical components [51]. Tseng *et al.* reported a lens-free holographic microscope attached to a cellphone with a spatial resolution of $1.5 \sim 2\ \mu\text{m}$ over a FOV of $\sim 24\ \text{mm}^2$ [52]. The additional hardware (~ 38 grams) installed on the cellphone is composed of an inexpensive LED (at 587 nm) with an aperture of $\sim 100\ \text{mm}$ in front of the light source.

The development in smartphone-based microscopy greatly strengthens and expands the capability of smartphone in POC diagnosis, especially in direct specimen examination. Microscale imaging opens an avenue for



Fig. 4. Direct tube, strip, and specimen inspection for POC diagnostics. (a) Smartphone-based health sweat and saliva biomarker detection device [55]. (b) Different views of the smart RDT reader prototype installed on an Android phone (Samsung Galaxy S II). This device can be repeatedly attached/detached to the cellphone body without the need for fine alignment and modification [56]. (c) A picture of the iTube platform, utilizing colorimetric assays and a smart phone-based digital reader for food allergen testing [58].

smartphone in POC diagnostics by granting it the power to directly examine bacteria, cells, and even viruses.

B. Smartphone-Based Strip, Tube, and Specimen Tests

Inspections of specimens directly, or by strips or tubes are the most commonly used diagnostic methods for many diseases [53]. In smartphone-based POC diagnostics, an image of the specimen, strip, or tube is captured first using the built-in camera or a converted microscopy as introduced in Section III-A. Then image postprocessing is used for counting targets or for colorimetric analysis in strip- and tube-based tests.

Smartphone-based microscopy can capture an image of a clinical specimen and further analyze it for target of interest. Breslauer’s group developed a smartphone-based microscope to image *P. falciparum*-infected sickle red

blood cells and *M. tuberculosis*-infected sputum samples and then automatically counted bacillus via image analysis [48]. Zhu *et al.* developed a compact smartphone microscopic platform to image blood samples, followed by the measurement of the density of blood cells and hemoglobin concentration through image processing [54].

Strip-based test results can be imaged using a smartphone’s built-in camera, followed by colorimetric analysis. Onescu’s group demonstrated an integrated smartphone accessory for monitoring changes in pH of sweat and salivary [Fig. 4(a)] [55]. This system consists of a smartphone case, a smartphone application, and disposable strips. The strip tested with sweat or saliva sample is inserted in a slot on the smartphone case and an image is taken. The pH is determined by checking the hue-pH correlation stored inside the application. Mudanyali *et al.* demonstrated a cellphone-based rapid-diagnostic-test (RDT) reader

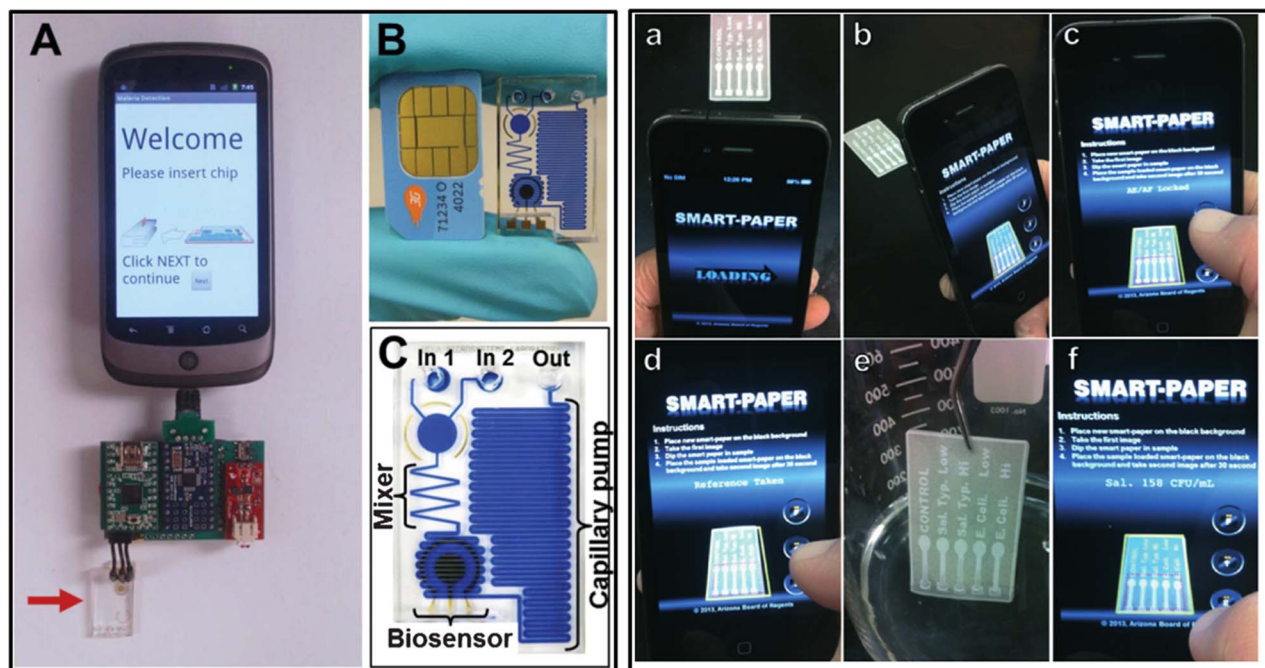


Fig. 5. Microfluidic based POC diagnostics. (Left) Photograph of the assembled prototype device for rapid electrochemical detection [18]. The arrow indicates the microfluidic chip. (Right) Smartphone application for *Salmonella* detection from a multichannel microfluidic device [69].

platform that can work with various lateral flow immunochromatographic assays [Fig. 4(b)] [56]. This device can be attached to a smartphone, and various types of test strips can be inserted in the device and imaged by the built-in camera of a smartphone. The captured raw image can be processed through an application for result analysis, and the result together with raw images can be transmitted to a central server if necessary. Lee *et al.* presented a system for rapid quantification of vitamin D levels by evaluating serum samples with a test strip that allows colorimetric detection of 25-hydroxyvitamin D using a gold nanoparticle-based immunoassay [57].

Tube-based tests share a similar mechanism with strip-based ones. Coskun *et al.* built a food allergen testing platform that images and automatically analyses colorimetric assays performed in test tubes for sensitive and specific detection of allergens in food samples [see Fig. 4(c)] [58]. The test and control tubes are inserted from the side and are vertically illuminated by two separate LEDs. The transmission images of the sample and control tubes are digitally processed using a cellphone application. With a similar technique, they further demonstrated an Albumin Tester platform that images and analyzes fluorescent assays confined with disposable test tubes for sensitive and specific detection of albumin in urine [59].

C. Smartphone-Based Microfluidic Tests

Microfluidics-based biochemical testing technologies, which are designed to analyze small volumes of body

fluids, have been widely studied for POC diagnostics [60], [61]. Microfluidic devices, coupled with different functional units (e.g., pumps, valves, and reactors), can be integrated into a miniaturized analytical system and manipulate a small volume of fluids, which greatly reduces the consumption of samples and reagents, and the complexity of operation procedures [18], [19], [62]–[64]. Microfluidic techniques can also integrate various assays into one single device to achieve multiplex assays, which greatly expands the capability, reduces the cost, and simplifies the operation of microfluidic tests.

Lillehoj's group developed a compact smartphone platform for rapid biomolecular detection [Fig. 5(a)], which consists of an embedded circuit for signal processing and disposable microfluidic chips for biosensing [18]. After the completion of each measurement, the results are displayed on the screen for immediate assessment, and automatically saved to the phone's memory for future analysis and transmission. The whole procedure can be carried out with two loading steps and takes 15 minutes to complete one measurement.

Stedtfeld *et al.* presented an inexpensive, user-friendly, and compact device operated on an iPod Touch (termed Gene-Z) for rapid diagnosis of multiple genetic markers [65]. It uses a disposable valve-less polymer microfluidic chip that contains four arrays with 15 reactions, each with dehydrated primers for isothermal amplification. This system is capable of simultaneous analysis of four samples for the detection of multiple

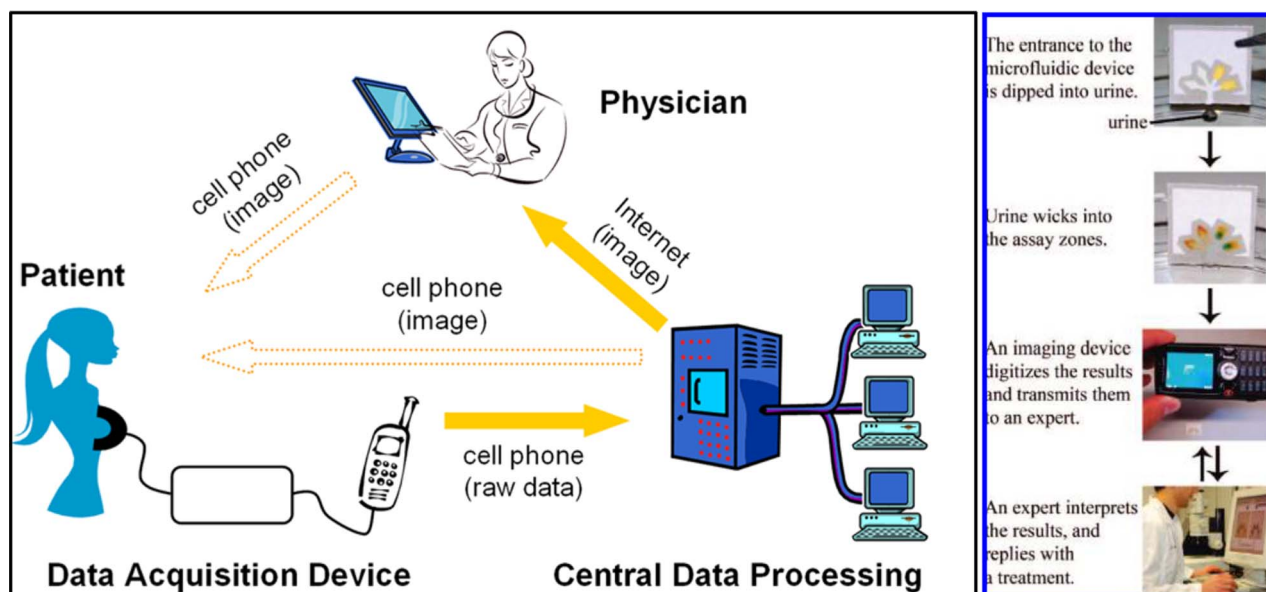


Fig. 6. Examples of smartphone-based telemedicine diagnostics. (Left) System configuration for the breast cancer tumors patient self-test screening [77]. (Right) General strategy for performing inexpensive bioassays in remote locations and for exchanging assay results to off-site technicians [78].

genetic markers, requiring only a single pipetting step per sample.

Besides the traditional chip-based microfluidic device discussed above, paper-based microfluidic devices are also widely used in smartphone-based POC diagnostics. Paper-based microfluidics is based on patterning sheets of paper with hydrophilic channels bounded by hydrophobic barriers, which are more cost-effective, sensitive, specific, and robust, thereby offering great advantages for developing POC diagnostics [66], [67]. Martinez *et al.* introduced a low-cost healthcare system that integrates paper-based microfluidics with camera-equipped cellular phones [68]. The results can be captured with a camera phone and transmitted to a central laboratory. Park *et al.* reported a smartphone-based *Salmonella* detection on paper microfluidics [69], [70]. The reaction result is quantified by taking digital images of the microfluidic device with a smartphone camera and implementing image-processing algorithms to calculate and display the bacterial concentration on the smartphone [see Fig. 5(b)]. The detection limit is down to a single cell level, and the total assay time is less than one minute.

IV. SMARTPHONE IN TELEMEDICINE

Today's smartphones are able to not only provide convenient and fast near-patient healthcare, but also facilitate long distance communication between on-site patients and off-site health centers with its powerful transmission ability [71], [72]. Therefore, in cases where off-site diagnosis and decision-making is needed, smartphone can collect

on-site disease data, transmit it to a health center, and receive analytical results [73]–[76]. Granot *et al.* reported a telemedicine system that physically separated the imaging, display, and analysis parts in a medical imaging system [Fig. 6(a)] [77]. This system consists of a medical imaging data acquisition device (DAD) at the patient site, a smartphone, and image reconstruction system at health center. The cell phone serves as a conduit between DAD at the patient site and the image reconstruction system.

Martinez *et al.* reported a smartphone system for the rapid quantification of bioassays and the exchange of assay results with off-site physicians [78]. This system used paper-based microfluidics to run multiple assays simultaneously and used camera phones to capture image results. The digital information was then transferred from on-site patient to off-site clinicians for analysis and the diagnosis result is transferred back via a cell phone [see Fig. 6(b)]. AirStrip Technologies developed a smartphone application that can obtain patient physiological data (e.g., ECG/EKG data, fetal heartbeat and maternal contraction patterns) collected by bedside monitoring equipment, and transmit it to health professionals in near real-time [79]. Gonzalez *et al.* reported a smartphone technique that can work in medically underserved regions in Mexico to detect intraperitoneal bleeding [80]. In this paradigm, electromagnetic coils were used to take bulk data from a magnetic field at the patient site. The data were then transmitted through a cellular phone to a central location that could process the raw data and return the diagnostic results to the patient site in real time.

V. DISCUSSION AND FUTURE PERSPECTIVES

Smartphone-based POC diagnostics offers great opportunities for delivering healthcare to resource-limited settings. Despite the increasing popularity, smartphone-based POC diagnostics faces some unsolved issues. The main concern centers on the reliability of POC testing procedure and the security of diagnostic results. For example, technologies intended to be used for POC diagnostics should be operable for the elderly, people with low literacy, and those with permanent or temporary disabilities [27]. The result indicated by smartphone applications should be explicit and nonmisleading. The management of personal health-related data, including data capturing, storage, up-linking to a server, and transmitting it through internet, should be secure and confidential.

We envision that the future development of smartphone-based POC diagnostics will focus on the following aspects. One aspect is the development of various types of portable biosensors that can be connected to a smartphone. For example, connecting a blood pressure meter to a smartphone, which is used for procedure control and result display, can create a simple sphygmomanometer.

REFERENCES

- W. Hersh, J. A. Jacko, R. Greenes, J. Tan, D. Janies, P. J. Embi, and P. R. O. Payne, "Health-care hit or miss?" *Nature*, vol. 470, no. 7334, pp. 327–329, Feb. 2011.
- R. Bercich, J. Bernhard, K. Larson, and J. Lindsey, "Hand-held plasma isolation device for point-of-care testing," *IEEE Trans. Biomed. Eng.*, vol. 58, no. 3, pp. 759–762, Mar. 2011.
- C. Greenhill, "Diagnosis: A new low-cost point-of-care test for liver function has been developed," *Nat. Rev. Gastroenterol. Hepatol.*, vol. 9, no. 618, 2012.
- N. R. Pollock, J. P. Rolland, S. Kumar, P. D. Beattie, S. Jain, F. Noubary, V. L. Wong, R. A. Pohlmann, U. S. Ryan, and G. M. Whitesides, "A paper-based multiplexed transaminase test for low-cost, point-of-care liver function testing," *Sci. Transl. Med.*, vol. 4, no. 152, 2012.
- E. Wang, D. J. Meier, R. M. Sandoval, V. E. Von Hendy-Willson, B. M. Pressler, R. M. Bunch, M. Alloosh, M. S. Sturek, G. J. Schwartz, and B. A. Molitoris, "A portable fiberoptic ratiometric fluorescence analyzer provides rapid point-of-care determination of glomerular filtration rate in large animals," *Kidney Int.*, vol. 81, no. 1, pp. 112–117, Jan. 2012.
- F. B. Myers and L. P. Lee, "Innovations in optical microfluidic technologies for point-of-care diagnostics," *Lab Chip*, vol. 8, no. 12, pp. 2015–2031, Dec. 2008.
- C. H. Ahn, J.-W. Choi, G. Beaucage, J. H. Nevin, J. Lee, A. Puntambekar, and J. Y. Lee, "Disposable Smart Lab on a Chip for Point-of-Care Clinical Diagnostics," *Proc. IEEE*, vol. 92, no. 1, pp. 154–173, Jan. 2004.
- S. C. Kazmierczak, "Point-of-care testing quality: Some positives but also some negatives," *Clin. Chem.*, vol. 57, no. 9, pp. 1219–1220, Sep. 2011.
- S. Wang, F. Xu, and U. Demirci, "Advances in developing HIV-1 viral load assays for resource-limited settings," *Biotechnol. Adv.*, vol. 28, no. 6, pp. 770–781, 2010.
- F. R. Beyette, C. A. Gaydos, G. J. Kost, and B. H. Weigl, "Point-of-Care Technologies for Health Care," *IEEE Trans. Biomed. Eng.*, vol. 58, no. 3, pp. 732–735, Mar. 2011.
- V. Gubala, L. F. Harris, A. J. Ricco, M. X. Tan, and D. E. Williams, "Point of care diagnostics: Status and future," *Anal. Chem.*, vol. 84, no. 2, pp. 487–515, Jan. 2012.
- J. Wang, "Electrochemical biosensors: Towards point-of-care cancer diagnostics," *Biosens. Bioelectron.*, vol. 21, no. 10, pp. 1887–1892, Apr. 2006.
- D. Huckle, "Point-of-care diagnostics: An advancing sector with nontechnical issues," *Expert Rev. Mol. Diagn.*, vol. 8, no. 6, pp. 679–688, Nov. 2008.
- R. McNerney and P. Daley, "Towards a point-of-care test for active tuberculosis: Obstacles and opportunities," *Nat. Rev. Microbiol.*, vol. 9, no. 3, pp. 204–213, Mar. 2011.
- A. Tefferi and J. W. Vardiman, "Classification and diagnosis of myeloproliferative neoplasms: The 2008 World Health Organization criteria and point-of-care diagnostic algorithms," *Leukemia*, vol. 22, no. 1, pp. 14–22, Jan. 2008.
- J. Yao, R. Schmitz, and S. Warren, "A wearable point-of-care system for home use that incorporates plug-and-play and wireless standards," *IEEE Trans. Inf. Technol. Biomed.*, vol. 9, no. 3, pp. 363–371, Sep. 2005.
- H. J. Lambers Heerspink, E. C. Witte, S. J. L. Bakker, P. E. de Jong, D. de Zeeuw, and R. T. Gansevoort, "Screening and monitoring for albuminuria: The performance of the HemoCue point-of-care system," *Kidney Int.*, vol. 74, no. 3, pp. 377–383, Aug. 2008.
- P. B. Lillehoj, M. Huang, N. Truong, and C. Ho, "Rapid electrochemical detection on a mobile phone," *Lab Chip*, pp. 2950–2955, 2013.
- D. C. Duffy, J. C. McDonald, O. J. Schueller, and G. M. Whitesides, "Rapid Prototyping of Microfluidic Systems in Poly(dimethylsiloxane)," *Anal. Chem.*, vol. 70, no. 23, pp. 4974–4984, Dec. 1998.
- R. Hawkins, "Managing the pre- and post-analytical phases of the total testing process," *Clin. Chem.*, vol. 32, no. 1, pp. 5–16, Jan. 2012.
- M. Eisenstein, "Miniature wireless sensors presage smart phone medicine," *Nat. Biotechnol.*, vol. 30, no. 11, pp. 1013–1014, 2012.
- International Data Corporation, "Worldwide Smartphone Shipments Top One Billion Units for the First Time, According to IDC, 2014." [Online]. Available: <https://www.idc.com/getdoc.jsp?containerId=prUS24645514>
- International Data Corporation, "Despite a Strong 2013, Worldwide Smartphone Growth Expected to Slow to Single Digits by 2017, According to IDC, 2014." [Online]. Available: <http://www.idc.com/getdoc.jsp?containerId=prUS24701614>
- N. D. Lane, E. Miluzzo, H. Lu, D. Peebles, T. Choudhury, and A. T. Campbell, "A survey of mobile phone sensing," *IEEE Commun. Mag.*, pp. 140–150, 2010.
- L. Mertz, "Ultrasound? Fetal Monitoring? Spectrometer? There's an app for that!" *IEEE Pulse*, pp. 16–21, 2012.
- J. Gold, "FDA Regulators Face Daunting Task as Health Apps Multiply," in *USA Today*. [Online]. Available: <http://usatoday30.usatoday.com/news/health/story/2012-06-22/health-apps-regulation/55766260/1>
- K. Patrick, W. Griswold, F. Raab, and S. S. Intille, "Health and the Mobile Phone," *Amer. J. Preview Med.*, vol. 35, no. 2, pp. 177–181, 2008.
- H. Wang and J. Liu, "Mobile phone based health care technology," *Recent Pat. Biomed. Eng.*, vol. 2, pp. 15–21, 2009.
- Q.-M. Xie and J. Liu, "Mobile Phone Based Biomedical Imaging Technology: A Newly

- Emerging Area," *Recent Patents Biomed. Eng.*, vol. 3, no. 1, pp. 41–53, Jan. 2010.
- [30] E. Agu, P. Pedersen, D. Strong, B. Tulu, Q. He, L. Wang, and Y. Li, "The smartphone as a medical device: Assessing enablers, benefits and challenges," in *Proc. 2013 IEEE Int. Conf. Sensing, Commun. Netw.*, Jun. 2013, pp. 76–80.
- [31] A. Ozcan, "Mobile phones democratize and cultivate next-generation imaging, diagnostics and measurement tools," *Lab Chip*, 2014.
- [32] A. Pantelopoulos and N. G. Bourbakis, "A survey on wearable sensor-based systems for health monitoring and prognosis," *IEEE Trans. Syst. Man, Cybern. C Applicat. Rev.*, vol. 40, no. 1, pp. 1–12, Jan. 2010.
- [33] S. Wang and J. Liu, "Biometrics on mobile phone," in *InTech*, 2010.
- [34] E. Jonathan and M. Leahy, "Investigating a smartphone imaging unit for photoplethysmography," *Physiol. Meas.*, vol. 31, no. 11, pp. N79–N83, Nov. 2010.
- [35] A. Pal, A. Sinha, A. D. Choudhury, T. Chattopadhyay, and A. Viswanathan, "A robust heart rate detection using smart-phone video categories and subject descriptors," in *Proc. MobileHealth'13*, 2013, pp. 43–48.
- [36] C. G. Scully, J. Lee, J. Meyer, A. M. Gorbach, D. Granquist-Fraser, Y. Mendelson, and K. H. Chon, "Physiological parameter monitoring from optical recordings with a mobile phone," *IEEE Trans. Biomed. Eng.*, vol. 59, no. 2, pp. 303–306, Feb. 2012.
- [37] U. Kim, S. Ghanbari, A. Ravikumar, J. Seubert, and S. Figueira, "Rapid, affordable, point-of-care water monitoring via a microfluidic DNA sensor and a mobile interface for global health," *IEEE Trans. Eng. Heal. Med.*, vol. 1, July 2013.
- [38] T. S. Kim, G. Yoon, J. Lee, and S. Shin, "Method of extracting region of interest from tongue image and health monitoring method and apparatus using the tongue image," Europe, EP1450287A2, 2004.
- [39] T. Wadhawan, N. Situ, H. Rui, K. Lancaster, X. Yuan, and G. Zouridakis, "Implementation of the 7-point checklist for melanoma detection on smart handheld devices," in *Proc. IEEE Eng. Med. Biol. Soc.*, 2012.
- [40] T. Yoshimine, "Diagnostic system and portable telephone device," The United States, US20040109571, 2004.
- [41] E. C. Larson, M. Goel, G. Boriello, S. Heltshe, M. Rosenfeld, and S. N. Patel, "SpiroSmart: Using a microphone to measure lung function on a mobile phone," in *Proc. 2012 ACM Conf. Ubiquitous Comput.*, 2012, pp. 280–289.
- [42] S. Huang and J. Liu, "Mobile phone based liquid crystal thermal imaging method and its medical implementation," *Chinese J. Med. Instrum.*, vol. 34, no. 5, pp. 317–322, 2010.
- [43] A. H. Khandoker, J. Black, and M. Palaniswami, "Smartphone-based low cost oximeter photoplethysmography," in *Proc. 6th Int. Conf. Elec. Comput. Eng.*, Dec. 2010, pp. 18–20.
- [44] J. Wojtczak and P. Bonadonna, "Pocket mobile smartphone system for the point-of-care submandibular ultrasonography," *Amer. J. Emerg. Med.*, vol. 31, no. 3, pp. 573–577, Mar. 2013.
- [45] H. Zhu, S. O. Isikman, O. Mudanyali, A. Greenbaum, and A. Ozcan, "Optical imaging techniques for point-of-care diagnostics," *Lab Chip*, vol. 13, no. 1, pp. 51–67, Jan. 2013.
- [46] J. Balsam, M. Ossandon, Y. Kostov, H. A. Bruck, and A. Rasooly, "Lensless CCD-based fluorometer using a micromachined optical Söller collimator," *Lab Chip*, vol. 11, no. 5, pp. 941–949, Mar. 2011.
- [47] Z. J. Smith, K. Chu, A. R. Espenson, M. Rahimzadeh, A. Gryshuk, M. Molinaro, D. M. Dwyre, S. Lane, D. Matthews, and S. Wachsmann-Hogiu, "Cell-phone-based platform for biomedical device development and education applications," *PLoS One*, vol. 6, no. 3, Jan. 2011.
- [48] D. N. Breslauer, R. N. Maamari, N. A. Switz, W. A. Lam, and D. A. Fletcher, "Mobile phone based clinical microscopy for global health applications," *PLoS One*, vol. 4, no. 7, 2009.
- [49] H. Zhu, O. Yaglidere, T. Su, D. Tseng, and A. Ozcan, "Cost-effective and compact wide-field fluorescent imaging on a cell-phone," *Lab Chip*, vol. 11, pp. 315–322, 2011.
- [50] Q. Wei, H. Qi, W. Luo, D. Tseng, S. J. Ki, Z. Wan, Z. Göröcs, L. A. Bentolila, T.-T. Wu, R. Sun, and A. Ozcan, "Fluorescent imaging of single nanoparticles and viruses on a smart phone," *ACS Nano*, vol. 7, no. 10, pp. 9147–9155, Oct. 2013.
- [51] A. Greenbaum, W. Luo, T. Su, Z. Göröcs, L. Xue, S. O. Isikman, A. F. Coskun, O. Mudanyali, and A. Ozcan, "Imaging without lenses: Achievements and remaining challenges of wide-field on-chip microscopy," *Nat. Methods*, vol. 9, no. 9, pp. 889–895, 2012.
- [52] D. Tseng, O. Mudanyali, C. Oztoprak, S. O. Isikman, I. Sencan, O. Yaglidere, and A. Ozcan, "Lensfree microscopy on a cellphone," *Lab Chip*, vol. 10, no. 14, pp. 1787–1792, Jul. 2010.
- [53] J. Hu, L. Wang, F. Li, Y. L. Han, M. Lin, T. J. Lu, and F. Xu, "Oligonucleotide-linked gold nanoparticle aggregates for enhanced sensitivity in lateral flow assays," *Lab Chip*, vol. 13, no. 22, pp. 4352–4357, Nov. 2013.
- [54] H. Zhu, I. Sencan, J. Wong, S. Dimitrov, D. Tseng, K. Nagashima, and A. Ozcan, "Cost-effective and rapid blood analysis on a cell-phone," *Lab Chip*, vol. 13, no. 7, pp. 1282–1288, Apr. 2013.
- [55] V. Oncescu, D. O'Dell, and D. Erickson, "Smartphone based health accessory for colorimetric detection of biomarkers in sweat and saliva," *Lab Chip*, vol. 13, pp. 3232–3238, 2013.
- [56] O. Mudanyali, S. Dimitrov, U. Sikora, S. Padmanabhan, I. Navruz, and A. Ozcan, "Integrated rapid-diagnostic-test reader platform on a cellphone," *Lab Chip*, vol. 12, pp. 2678–2686, 2012.
- [57] S. Lee, V. Oncescu, M. Mancuso, S. Mehta, and D. Erickson, "A smartphone platform for the quantification of vitamin D levels," *Lab Chip*, vol. 14, no. 8, pp. 1437–1442, 2014.
- [58] A. F. Coskun, J. Wong, D. Khodadadi, R. Nagi, A. Tey, and A. Ozcan, "A personalized food allergen testing platform on a cellphone," *Lab Chip*, vol. 13, pp. 636–640, 2013.
- [59] A. F. Coskun, R. Nagi, K. Sadeghi, S. Phillips, and A. Ozcan, "Albumin testing in urine using a smart-phone," *Lab Chip*, vol. 13, no. 21, pp. 4231–4238, Aug. 2013.
- [60] S. Wang, S. Tasoglu, P. Z. Chen, M. Chen, R. Akbas, S. Wach, C. I. Ozdemir, U. A. Gurkan, F. F. Gigue, D. R. Kuritzkes, and U. Demirci, "Micro-a-fluidics ELISA for rapid CD4 cell count at the point-of-care," *Sci. Rep.*, vol. 4, p. 3796, Jan. 2014.
- [61] W. G. Lee, Y.-G. Kim, B. G. Chung, U. Demirci, and A. Khademhosseini, "Nano/microfluidics for diagnosis of infectious diseases in developing countries," *Adv. Durg Deliv Rev*, vol. 62, pp. 449–457, 2011.
- [62] D. C. Duffy, O. J. A. Schueller, S. T. Brittain, and G. M. Whitesides, "Rapid prototyping of microfluidic switches in poly (dimethyl siloxane) and their actuation by electroosmotic," *J. Micromechan.*, vol. 9, pp. 211–217, 1999.
- [63] M. A. Unger, H.-P. Chow, T. Thorsen, A. Scherer, and S. R. Quake, "Monolithic microfabricated valves and pumps by multilayer soft lithography," *Science*, vol. 288, no. 5463, pp. 113–116, Apr. 2000.
- [64] J. Hu, S. Wang, L. Wang, F. Li, B. Pinguan-Murphy, T. J. Lu, and F. Xu, "Advances in paper-based point-of-care diagnostics," *Biosens. Bioelectron.*, vol. 54, pp. 585–597, Apr. 2014.
- [65] R. D. Stedtfeld, D. M. Tourlousse, G. Seyrig, T. M. Stedtfeld, M. Kronlein, S. Price, F. Ahmad, E. Gulari, M. Tiedje, and S. A. Hashsham, "Gene-Z: A device for point of care genetic testing using a smartphone," *Lab Chip*, vol. 12, pp. 1454–1462, 2012.
- [66] A. Nilghaz, D. H. Wicaksono, D. Gustiono, F. A. Abdul Majid, E. Supriyanto, and M. R. Abdul Kadir, "Flexible microfluidic cloth-based analytical devices using a low-cost wax patterning technique," *Lab Chip*, vol. 12, pp. 209–218, 2012.
- [67] Y. L. Han, W. Wang, J. Hu, G. Huang, S. Wang, W. G. Lee, T. J. Lu, and F. Xu, "Benchtop fabrication of three-dimensional reconfigurable microfluidic devices from paper-polymer composite," *Lab Chip*, vol. 13, no. 24, pp. 4745–4749, Dec. 2013.
- [68] A. W. Martinez, S. T. Phillips, G. M. Whitesides, and E. Carrilho, "Diagnostics for the developing world: Microfluidic paper-based analytical devices," *Anal. Chem.*, vol. 82, no. 1, pp. 3–10, Jan. 2010.
- [69] T. S. Park, W. Li, K. E. McCracken, and J.-Y. Yoon, "Smartphone quantifies salmonella from paper microfluidics," *Lab Chip*, vol. 13, no. 24, pp. 4832–4840, Nov. 2013.
- [70] T. S. Park, W. Li, and J. Yoon, "Paper microfluidic detection of salmonella using a smart phone," in *Proc. 16th Int. Conf. Miniaturized Syst. Chem. Life Sci.*, 2012, pp. 2002–2004.
- [71] World Health Organization, Essential health technologies strategy 2004–2007. [Online]. Available: http://www.who.int/eh/eh/EHT_strategy_2004-2007
- [72] A. G. Ekeland, A. Bowes, and S. Flottorp, "Effectiveness of telemedicine: A systematic review of reviews," *Int. J. Med. Inform.*, vol. 79, no. 11, pp. 736–771, Nov. 2010.
- [73] J. L. Feder, "Cell-phone medicine brings care to patients in developing nations," *Health Aff.*, vol. 29, no. 2, pp. 259–263, Feb. 2010.
- [74] M. Moore, "The evolution of telemedicine," *Futur. Gener. Comput. Syst.*, vol. 15, no. 2, pp. 245–254, Mar. 1999.
- [75] T. Takahashi, "The present and future of telemedicine in Japan," *Int. J. Med. Inform.*, vol. 61, no. 2–3, pp. 131–137, May 2001.
- [76] S. Potthoff and D. Ph, "Home telehealth improves clinical outcomes at lower cost for home healthcare," *Telemed. e-Health*, vol. 12, no. 2, pp. 128–136, 2006.
- [77] Y. Granot, A. Ivorra, and B. Rubinsky, "A new concept for medical imaging centered on cellular phone technology," *PLoS One*, vol. 3, no. 4, pp. 1–7, 2008.
- [78] A. W. Martinez, S. T. Phillips, E. Carrilho, S. W. Thomas, H. Sindi, and G. M. Whitesides, "Simple telemedicine for developing regions: Camera phones and paper-based microfluidic devices for real-time, off-site diagnosis," *Anal. Chem.*, vol. 80, no. 10, pp. 3699–3707, May 2008.

[79] AirStrip, AirStrip ONE, Webpage, 2013. [Online]. Available: <http://www.airstriptechnology.com/airstrip-one>

[80] C. A. Gonzalez, G. Blumrosen, and B. Rubinsky, "Remote monitoring of internal bleeding based on magnetic induction and

cellular phone technology: A potential application in poor regions in México," *Comput. Syst.*, vol. 14, no. 2, pp. 187–195, 2010.

[81] S. Wang, X. Zhao, I. Khimji, R. Akbas, W. Qiu, D. Edwards, D. Cramer, B. Ye, and

U. Demirci, "Integration of cell phone imaging with microchip ELISA to detect ovarian cancer HE4 biomarker in urine at the point-of-care," *Lab Chip*, vol. 11, pp. 3411–3418, 2011.

ABOUT THE AUTHORS

Xiayu Xu received the Ph.D. degree in biomedical engineering from the University of Iowa, Iowa City, IA, USA, in 2012.

She worked as a postdoctoral research fellow at Iowa Institute of Biomedical Imaging (IIBI), the University of Iowa for one year, and she is currently an assistant professor at Xi'an Jiaotong University, China. Her main research interests focus on point-of-care diagnostic techniques, including microfluidics, optical imaging, and image postprocessing.



Altug Akay received the B.A. degree from the University of Massachusetts at Amherst in 2005, and the M.A. degree from Dartmouth College, Dartmouth, MA, USA. He is currently pursuing the Ph.D. degree in the School of Technology and Health at the Royal Institute of Technology in Stockholm, Sweden.



Upon graduating from Dartmouth, he worked at Siemens Healthcare, Erlangen, Germany, for one year under the supervision of Dr. Gudrun Zahlmann. He worked at Spaulding Rehabilitation Hospital under the supervision of Dr. Paolo Bonato from 2008 to 2009 and at the Bio-Acoustic MEMs in Medicine (BAMM) labs under the supervision of Dr. Utkan Demirci from 2010 to 2011. He also contributed a book chapter entitled " β -thalassemia's social and economic geography: a possible prevention/treatment program to rout "legacy" genetic mutations," in the book entitled *Mathematical Methods in Scattering Theory and Biomedical Engineering*, (London, U.K., World Scientific, 2008). His current interests are Global Healthcare, Point-of-Care Diagnostics, and Health Technology.

Huilin Wei, photograph and biography not available at the time of publication.

ShuQi Wang received the Ph.D. degree from the University of Cambridge, U.K., in 2009, focusing on rapid nucleic acid amplification technologies for HIV viral load monitoring in resource-limited settings.

Since then, he has been working on the development of point-of-care diagnostics at Harvard Medical School and Stanford School of Medicine. His recent work on the development of cell-phone based on-chip ELISA was featured as the front cover of *Lab on a Chip*.



Belinda Pingguan-Murphy received the Ph.D. degree in medical engineering from Queen Mary and Westfield College, University of London, London, U.K.

Currently, she is a senior lecturer in the Department of Biomedical Engineering, Faculty of Engineering, University of Malaya, Malaysia. She is also the program coordinator for the master of engineering program for the department. Her research interests include advanced biomaterials, tissue engineering, engineering cell microenvironments, mechanotransduction, stem cell technologies, and point of care.



Björn-Erik Erlandsson was born in 1949. He received the Ph.D. degree from Chalmers University of Technology, Gothenburg, Sweden, in the field of applied electronics.



Currently, he is a Senior Advisor, Professor at the School of Technology and Health, Royal Institute of Technology, Stockholm, Sweden, with responsibility for technology and quality in healthcare. Experience from research and development, quality management, and regulatory affairs from international medical device industry; Siemens and Nobel Industries. Worked as Quality Manager in pacemaker industry and has been Director in Medical Informatics and Technology at the University Hospital of Northern Sweden, Umeå and Akademiska Hospital, Uppsala and also professor in Biomedical Engineering. In his role as director for technical operations at the university hospitals, he has also been heavily involved in investment issues and investment management, and chairman of the investment planning groups.

He is also involved in the standardization work in medical technology and medical informatics, Chairman of SIS/TK334 and Head of the Swedish delegation to international standardization in CEN and ISO in Health Informatics, Chairman of the Joint Working Group in Software and Medical Devices (SAMd) at CEN/CENELEC. Board member of HL7 Sweden. Chairman of the Medical Society's Division of Medical Informatics for two years, member of the Swedish Council on Health Technology Assessment, SBU Alertråd, and Coordinator EU policies at the Royal Institute of Technology's Life Science Platform. He is also the Deputy Dean at the School of Technology and Health at the Royal Institute of Technology, Stockholm.

XiuJun Li received the Ph.D. degree in bioanalytical chemistry with Dr. Paul Li in 2008 from Simon Fraser University, Canada, and then moved to University of California Berkeley with Dr. Richard Mathies and Harvard University, Cambridge, MA, USA, with Dr. George Whitesides for his postdoctoral research from 2009 to 2011, as a NSERC Postdoctoral Fellow.



Currently, he is a tenure-track Assistant Professor in the Department of Chemistry, Border Biomedical Research Center (BBRC), Biomedical Engineering (BME), and Materials Science & Engineering (MASE) at University of Texas at El Paso (UTEP), USA. His current research interest is centered on bioanalysis and bioengineering using microfluidic lab-on-a-chip and nanosensing, including but not limited to low-cost diagnosis, hybrid microfluidic devices, single-cell analysis and 3D cell culture.

Dr. Li is the recipient of UT STARS Award in 2012, UTEP Outstanding Performance Award in 2014, and the 2014 Bioanalysis Young Investigator Award.

WonGu Lee received the Ph.D. degree in mechanical engineering from Seoul National University, Korea.

After finishing his doctoral studies, he was a Postdoctoral Researcher at Harvard-MIT Health Sciences and Technology, Harvard Medical School and Wyss Institute at Harvard University, Cambridge, MA, USA. He is currently an Associate Professor in the Department of Mechanical Engineering, Kyung Hee University, Korea. His research focuses on development of wearable healthcare devices for human rehabilitation and augmentation, and commercialization of point-of-care devices using cell manipulation in microfluidics.

Dr. Lee is also Founder and Chairman of Wearable Healthcare Inc., Korea.



Lin Wang received the B.S. degree in clinical medicine from Shanxi Medical University, Shanxi, China, in 2004, the M.S. degree in zoology from Jinan University, Guangdong, China, in 2006, the Ph.D. degree in Hydrobiology from Jinan University, Guangdong, China, in 2010, and worked as a Postdoctoral Fellow at the MOE Key laboratory of Biomedical Information Engineering, School of Life Science and Technology, and Bioinspired Engineering and Biomechanics center, Xi'an Jiaotong University, Shaanxi, China.

Currently, as a postdoc at Washington University School of Medicine in St. Louis, MO, USA, she is working on cardiomyocyte tissues engineering. Her research interests include cell responses to mechanical stimulus, paper based point-of-care diagnostics, microfluidic chip for point-of-care testing and biochemistry and molecular biology.



Jie Hu is pursuing the Ph.D. degree of biomedical engineering in School of Life Science and Technology and Bioinspired Engineering and Biomechanics Center, Xi'an Jiaotong University, Xi'an, Shaanxi, China.

His work has focused on the research and development of low-cost and rapid biochemical analytical devices based on microfluidics and nanotechnologies for disease diagnosis, environment monitoring, and food safety analysis.



Feng Xu received the Ph.D. degree in engineering from University of Cambridge, United Kingdom. Then, Dr. Xu worked as a research fellow at Harvard Medical School and Harvard-MIT Health Science & Technology (HST).

He founded the first interdisciplinary biomedical engineering center of Xi'an Jiaotong University (*XJTU Bioinspired Engineering & Biomechanics Center*) and is the cofounding director of the center. Currently, he is a full professor at Xi'an Jiaotong University, China. His current research aims at advancing human health through academic excellence in education and research that integrates engineering, science biology and medicine with focus on biothermomechanics, engineering of cell microenvironment, and point-of-care technologies.

